IMPORTANCE Ischemia is an important pathophysiological mechanism after traumatic brain injury (TBI), but its incidence and spatiotemporal patterns are poorly characterized.

OBJECTIVE To comprehensively characterize the spatiotemporal changes in cerebral physiology after TBI.

DESIGN, SETTING, AND PARTICIPANTS This single-center cohort study uses 15 oxygen positron emission tomography data obtained in a neurosciences critical care unit from February 1998 through July 2014 and analyzed from April 2018 through August 2019. Patients with TBI requiring intracranial pressure monitoring and control participants were recruited.

EXPOSURES Cerebral blood flow (CBF), cerebral blood volume (CBV), cerebral oxygen metabolism (CMRO₂), and oxygen extraction fraction.

MAIN OUTCOMES AND MEASURES Ratios (CBF/CMRO₂ and CBF/CBV) were calculated. Ischemic brain volume was compared with jugular venous saturation and brain tissue oximetry.

RESULTS A total of 68 patients with TBI and 27 control participants were recruited. Results from 1 patient with TBI and 7 health volunteers were excluded. Sixty-eight patients with TBI (13 female [19%]; median [interquartile range] age, 29 [22-47] years) underwent 90 studies at early (day 1 [n = 17]), intermediate (days 2-5 [n = 54]), and late points (days 6-10 [n = 19]) and were compared with 20 control participants (5 female [25%]; median [IQR] age, 43 [31-47] years). The global CBF and CMRO₂ findings for patients with TBI were less than the ranges for control participants at all stages (median [IQR]: CBF, 26 [22-30] mL/100 mL/min vs 38 [29-49] mL/100 mL/min; P < .001; CMRO₂, 62 [55-71] μmol/100 mL/min vs 131 [101-167] μmol/100 mL/min; P < .001). Early CBF reductions showed a trend of high oxygen extraction fraction (suggesting classical ischemia), but this was inconsistent at later phases. Ischemic brain volume was elevated even in the absence of intracranial hypertension and highest at less than 24 hours after TBI (median [IQR], 36 [10-82] mL), but many patients showed later increases (median [IQR] 6-10 days after TBI, 24 [4-42] mL; across all points: patients, 10 [5-39] mL vs control participants, 1 [0-3] mL; P < .001). Ischemic brain volume was a poor indicator of jugular venous saturation and brain tissue oximetry. Patients’ CBF/CMRO₂ ratio was higher than controls (median [IQR], 0.42 [0.35-0.49] vs 0.3 [0.28-0.33]; P < .001) and their CBF/CBV ratio lower (median [IQR], 7.1 [6.4-7.9] vs 12.3 [11.0-14.0]; P < .001), suggesting abnormal flow-metabolism coupling and vascular reactivity. Patients’ CBV was higher than controls (median [IQR], 3.7 [3.4-4.1] mL/100 mL vs 3.0 [2.7-3.6] mL/100 mL; P < .001), although values were lower in patients with intracranial hypertension; these were still greater than controls (median [IQR], 3.7 [3.2-4.0] vs 3.0 [2.7-3.6] mL/100 mL; P = .002), despite more profound reductions in partial pressure of carbon dioxide (median [IQR], 4.3 [4.1-4.6] kPa vs 4.7 [4.3-4.9] kPa; P < .001).

CONCLUSIONS AND RELEVANCE Ischemia is common early, detectable up to 10 days after TBI, possible without intracranial hypertension, and inconsistently detected by jugular or brain tissue oximetry. There is substantial between-patient and within-patient pathophysiological heterogeneity; ischemia and hyperemia commonly coexist, possibly reflecting abnormalities in flow-metabolism coupling. Increased CBV may contribute to intracranial hypertension but can coexist with abnormal CBF/CBV ratios. These results emphasize the need to consider cerebrovascular pathophysiological complexity when managing patients with TBI.

Published online November 11, 2019.

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Outcome after traumatic brain injury (TBI) is associated with not only initial injury severity but also secondary insults, including ischemia, brain swelling, and intracranial hypertension. Changes in cerebrovascular physiology after TBI contribute to all of these insults. Ensuring that cerebral blood flow (CBF) is adequate for oxygen and substrate delivery represents a fundamental management aim, which is pursued by optimizing cerebral perfusion pressure (CPP) and ventilation and controlling intracranial pressure (ICP).

The physiology that underpins these aims and therapies used to achieve them are incompletely understood. Many studies have measured CBF without reference to regional cerebral oxygen metabolism (CMRO₂), making it difficult to distinguish ischemia from CBF appropriately coupled to reduced metabolism and neuronal loss. Where studies have measured CMRO₂, sample sizes have been small and do not cover the dynamic temporal and spatial evolution of cerebrovascular pathophysiology. Further, many studies have concentrated on physiology within lesions and have not examined regions that initially appear structurally normal.

While brain swelling and ICP elevation drive up to half of TBI-associated mortality and remain therapeutic targets, the underlying physiology is unclear. Studies suggest that intracranial hypertension is predominantly attributable to brain edema, with cerebral blood volume (CBV) playing a limited role. However, in these studies, CBV was indirectly calculated rather than directly measured. These issues are important, since ICP-lowering therapies have competing benefits and harms. For example, lowering the partial pressure of carbon dioxide (PaCO₂) reduces vascular caliber and hence CBV and ICP, but it also reduces CBF, increasing the risk of ischemia.

While cerebrovascular physiology can be assessed with several imaging techniques, ⁴¹⁵O oxygen positron emission tomography (⁴¹⁵O PET) is the current reference standard for CBF, CBV, CMRO₂, and oxygen extraction fraction (OEF). While results from multiple centers have been integrated, this is hampered by differences in PET methodology (e.g., bolus vs steady-state techniques) and approaches to data analysis (e.g., voxel-based vs region-of-interest analysis). There remains a need for comprehensive characterization of cerebrovascular physiology after TBI using standardized ¹⁵O PET in a large patient sample across the full temporal disease narrative.

We aimed to comprehensively characterize cerebrovascular physiology within brain regions that initially appear structurally normal, using standardized ¹⁵O PET in a large patient cohort up to 10 days after TBI. We describe temporal changes in physiology, document changes in flow-metabolism coupling (CBF/CMRO₂) and local microvascular flow-volume associations (CBF/CBV), disentangle ischemia from coupled hypoperfusion, and assess the contribution of vascular engorgement to ICP elevation.

Methods

Additional details are provided within the eMethods in the Supplement. Control participants and patients with TBI requiring ICP monitoring within intensive care underwent ¹⁵O PET between February 1998 and July 2014. We excluded technically inadequate imaging studies and those with large variations of arterial pressure or PaCO₂. Some data have been reported previously, but none for the aims of the current article.

Studies were approved by the Cambridgeshire Research Ethics Committee and UK Administration of Radioactive Substances Advisory Committee and conducted in accordance with 1964 Declaration of Helsinki and later amendments. Volunteers provided informed consent, and assent was obtained from patient representatives, with patient consent obtained at follow-up if capacity was regained.

Clinical Protocols

Patients

Protocol-driven therapy targeted an ICP of less than 20 mm Hg and a CPP of 60 to 70 mm Hg, as described by Menon. Mechanical ventilation and tight control of respiratory and cardiovascular physiology during PET studies with (where available) PaCO₂ reductions titrated against jugular venous saturation (SJV O₂) and brain-tissue oximetry (BTPO₂). Outcomes were recorded using the Glasgow Outcome Score (GOS) at 6 months after TBI.

Imaging

Maps of CBF, CBV, CMRO₂, and OEF were calculated as previously described after PET, using a General Electric Advance scanner (GE Medical Systems) at the Wolfson Brain Imaging Centre of the University of Cambridge (Cambridge, United Kingdom). We categorized studies into 3 groups: within 24 hours of TBI (early), 2 to 5 days after TBI (intermediate), and 6 to 10 days after TBI (late).

Image Analysis

This analysis used whole-brain and standardized regions of interest (ROIs), excluding regions with lesions identified on registered computed tomography or magnetic resonance imaging. To account for pathophysiological heterogeneity within ROIs and assess ischemic burden, we estimated an individualized critical OEF threshold using a previously validated technique. Calculation of the volume of voxels with OEF greater than this...
threshold allowed estimation of the ischemic brain volume (IBV). We plotted IBV against SJVO\textsubscript{2} and BTPO\textsubscript{2} to identify thresholds for critical ischemia.

We calculated CBF/CMRO\textsubscript{2} to assess the efficiency of flow-metabolism coupling and CBF/CBV as an index of local CPP.\textsuperscript{30,31} To determine whether differences in CBF/CBV represented intrinsic differences in vascular physiology or CPP variance, we calculated CBF/CBV divided by CPP.

Statistical Analysis

Because data were not normally distributed, results are expressed as median (interquartile range [IQR]), and we used non-parametric statistical tests within R version 3.5.2 (R Foundation for Statistical Computing). In addition, we undertook linear mixed-effects regression of log-transformed PET parameters, adjusting for ROI, to analyze the difference in regional physiology between patients with TBI and healthy control participants, and we added time as a covariate (linear and quadratic to allow for nonlinear effects) to examine the association of time with changes in cerebrovascular physiology. We compared models with and without these terms using χ² tests. Correlation coefficients were calculated using Spearman rank tests, and Mann-Whitney tests were used when comparing patients and control participants. For comparisons between groups, we used the Kruskal-Wallis test with the Dunn test for post hoc comparisons. Linear plots were used to help visualize the associations between parameters.

For between-group comparisons of basic demographic and clinical data, a P value of .05 or less was regarded as significant. Additional results were interpreted taking into consideration that, to infer statistical significance, a Bonferroni correction for 7 variables (CBF, CBV, CMRO\textsubscript{2}, OEF, CBF/CMRO\textsubscript{2}, CBF/CBV, and IBV) would require \( P < .007 \), and for regional comparisons (14 ROIs), \( P < 5.0 \times 10^{-4} \) would be required. We also sought associations between IBV and GOS stratified for time after injury to replicate a previous finding\textsuperscript{4} in the early phase after TBI.

Results

A total of 27 control participants and 68 patients with TBI were recruited; imaging studies from 7 control participants and 1 study from 1 patient with TBI were excluded because of poor quality. We analyzed data from 20 control participants with no clinically significant neurological or psychiatric illness and 90 PET sessions in 68 patients with TBI with stable physiology during imaging (eFigure 1 in the Supplement).

Included patients had severe TBI (Glasgow Coma Scale score ≤8 on admission) or presented with moderate TBI (Glasgow Coma Scale score, 9-12) and subsequently deteriorated. Of the 90 PET studies, 17 were within 24 hours of the TBI (early), 54 between 2 and 5 days after the TBI (intermediate), and 19 after 6 or more days after the TBI (late). Seventeen patients had PET studies on more than 1 occasion, but only 3 had studies at all 3 times. Table 1 summarizes the baseline demographics and physiology during imaging (median [IQR] age: control participants, 43 [31-47] years; patients with TBI, 29 [22-47] years; female participants: control participants, 5 of 20 [25%]; patients with TBI, 13 of 55 [19%]).

Patients had lower CPP (median [IQR], 73[70-80] vs 81[75-88]; \( P = .008 \)) and PaCO\textsubscript{2} (median [IQR], 4.6 [4.2-4.8] kPa vs 5.6 [5.2-5.7] kPa; \( P < .001 \)) than control participants. With the exception of CPP, which was significantly higher in the TBI group with late imaging compared with those with intermediate imaging (median [IQR] values, 80 [77-91] vs 73 [69-78] mm Hg; \( P = .008 \); Table 1), there were no differences in physiological variables (hemoglobin, PaO\textsubscript{2}, PaCO\textsubscript{2}, and ICP) between the different TBI groups. Despite attempted management to a target ICP of 20 mm Hg or less, this was not achieved in all patients; 9 patients had ICP levels of 25 mm Hg or more during imaging.

Global Physiology

Patients, compared with control participants, had lower CBF (median [IQR], 26 [22-30] mL/100 mL/min vs 38 [29-49] mL/100 mL/min; \( P < .001 \)) and CMRO\textsubscript{2} (median [IQR], 62 [55-71] μmol/100 mL/min vs 131 [101-167] μmol/100 mL/min; \( P < .001 \)) and higher CBV (median [IQR], 3.7 [3.4-4.1] mL/100 mL vs 3.0 [2.7-3.6] mL/100 mL; \( P < .001 \)) despite lower PaCO\textsubscript{2} (median [IQR], 4.6 [4.2-4.8] kPa vs 5.6 [5.2-5.7] kPa; \( P < .001 \)). The CBF/CMRO\textsubscript{2} ratio was higher in patients (median [IQR], 0.42 [0.35-0.49] vs 0.3 [0.28-0.33]; \( P < .001 \)), while CBF/CBV was lower (median [IQR], 7.1 [6.4-7.9] vs 12.3 [11.0-14.0]; \( P < .001 \)). The difference in OEF between patients and control participants (median [IQR], 39% [35%-43%] vs 44% [40%-45%]; \( P = .02 \)) did not survive correction for multiple comparisons but was significantly lower at the intermediate point (median [IQR], 38% [32%-42%]; \( P = .004 \); Table 2). Compared with the rest of the group, physiology in patients who underwent craniectomy was similar to those who did not, while barbiturate coma was associated with lower CMRO\textsubscript{2} (median [IQR], 53 [43-64] μmol/100 mL/min vs 65 [57-74] μmol/100 mL/min; \( P = .004 \)), but reductions in CBF (median [IQR], 21 [18-27] mL/100 mL vs 27 [23-32] mL/100 mL; \( P = .01 \)) and CBV (median [IQR], 3.2 [3.1-4.3] mL/100 mL vs 3.8 [3.4-4.1] mL/100 mL; \( P = .03 \)) did not remain significant after correction for multiple comparisons.

Regional Physiology

Spatial heterogeneity was obvious on imaging (Figure 1), with regional variability shown across the whole-brain ROI template (eFigure 2 in the Supplement) both within and between patients, compared with control participants (eTables 1 and 2 and eFigure 3 in the Supplement). Using a linear mixed-effects regression model comparing affected patients with control participants, regional CBF, CBV, and CMRO\textsubscript{2} in patients were found to be significantly different (covariate effect estimates, −0.37, 0.16, and −0.71, respectively; all comparisons \( P < .001 \)), while OEF (covariate effect estimate, −0.12; \( P = .01 \)) did not remain significant after correction for multiple comparisons. There were also significant differences between control participants and patients at various points after injury (eTable 3 in the Supplement), and the time-dependent models for CBF, CBV, CMRO\textsubscript{2}, and OEF fit the data significantly better (−0.85, −0.39, 0.72, and 0.9 for standardized time, and 0.17, 0.09, −0.23, and 0.25 for standardized time).
Time^2, respectively; all comparisons, P < .001. Temporal trends differed between patients and control participants (Figure 2): CBF was low, showed a transient recovery, and then decreased again, while CMRO\textsubscript{2} was initially low and decreased further over time. Oxygen extraction fraction was initially high and fell in the intermediate period before trending toward

<table>
<thead>
<tr>
<th>Table 1. Baseline Demographics and Physiology During Imaging</th>
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<tbody>
<tr>
<td><strong>Characteristic</strong></td>
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<tr>
<td></td>
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<tr>
<td>Age, y</td>
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<td>Sex</td>
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<td>Female</td>
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<td>Male</td>
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<td>Postresuscitation Glasgow Coma Scale score</td>
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<td>V</td>
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<td>VI</td>
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<td>Primary lesion</td>
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<td>Extradural hematoma</td>
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<tr>
<td>Subdural hematoma</td>
</tr>
<tr>
<td>Contusion</td>
</tr>
<tr>
<td>Diffuse axonal injury</td>
</tr>
<tr>
<td>Intracranial pressure, mm Hg\textsuperscript{e}</td>
</tr>
<tr>
<td>Cerebral perfusion pressure, mm Hg\textsuperscript{e}</td>
</tr>
</tbody>
</table>

Abbreviations: IQR, interquartile range; NA, not applicable; TBI, traumatic brain injury.

SI conversaion factor: To convert hemoglobin to g/L, multiply by 1.0.0.

\* Mann-Whitney test between all patients with TBI and control participants.

\* Within 24 hours of traumatic brain injury.

\* Two to 5 days after traumatic brain injury.

\* Six to 10 days after traumatic brain injury.

\* Kruskal-Wallis test between all groups, with subsequent comparisons made between each TBI group and control participants using the post hoc Dunn test.

\* Marshall Score: diffuse injury (I-IV), evacuated mass lesion (V), and nonevacuated mass lesion (VI).

\* P < .001; P values less than .05 were considered significant.

\* Intracranial pressure, cerebral perfusion pressure, partial pressure of oxygen, and partial pressure of carbon dioxide in individual imaging studies are the mean values of these variables over the course of each positron emission tomography study.

\* In control participants, cerebral perfusion pressure was defined assuming an intracranial pressure of 11 mm Hg.

\* P = .04; P values less than .05 were considered significant.

\* P = .09; P values less than .05 were considered significant.

\* In this group, 3 patients were missing data.
normal values. Cerebral blood volume showed less variation and cerebral blood volume showed less variation and showed a trend for higher values than normal at all points. The 17 patients who underwent PET on more than 1 occasion showed a pattern similar to the overall cohort (eTable 4 and eFigure 4 in the Supplement).

**Flow Metabolism Coupling**

Wide variations in OEF (which imply large variations in flow-metabolism coupling) and regions with particularly low OEF (implying hyperemia) were common and most prominent between days 2 through 5 (Figure 2 and eFigure 3 within the Supplement). These abnormalities in CBF/CMRO₂ ratios were

### Table 2. Temporal Pattern of Global Physiological Derangements

<table>
<thead>
<tr>
<th>Positron Emission Tomography Sessions</th>
<th>Median (IQR)</th>
<th>P Value*</th>
<th>Patients With TBI, Median (IQR)</th>
<th>P Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Positron Emission Tomography Sessions</td>
<td>Control Participants (n = 20)</td>
<td>TBI (n = 90)</td>
<td>Early (n = 17)</td>
<td>Intermediate (n = 54)</td>
</tr>
<tr>
<td>Cerebral blood flow, mL/100 mL/min</td>
<td>38 (29-49)</td>
<td>26 (22-30)</td>
<td>.&lt;.001</td>
<td>25 (24-30)</td>
</tr>
<tr>
<td>Cerebral blood volume, mL/100 mL</td>
<td>3.0 (2.7-3.6)</td>
<td>3.7 (3.4-4.1)</td>
<td>.&lt;.001</td>
<td>3.6 (3.3-3.9)</td>
</tr>
<tr>
<td>Cerebral oxygen metabolism, μmol/100 mL/min</td>
<td>131 (101-167)</td>
<td>62 (55-71)</td>
<td>.&lt;.001</td>
<td>76 (70-85)</td>
</tr>
<tr>
<td>Oxygen extraction fraction, %</td>
<td>44 (40-45)</td>
<td>39 (35-43)</td>
<td>.02</td>
<td>46 (41-52)</td>
</tr>
<tr>
<td>Cerebral blood flow–cerebral oxygen metabolism ratio</td>
<td>0.30 (0.28-0.33)</td>
<td>0.42 (0.35-0.49)</td>
<td>.&lt;.001</td>
<td>0.35 (0.28-0.39)</td>
</tr>
<tr>
<td>Cerebral blood flow–cerebral blood volume ratio</td>
<td>12.3 (11.0-14.0)</td>
<td>7.1 (6.4-7.9)</td>
<td>.&lt;.001</td>
<td>7.2 (6.8-7.7)</td>
</tr>
<tr>
<td>Ischemic brain volume, mL</td>
<td>1 (0-3)</td>
<td>10 (5-39)</td>
<td>.&lt;.001</td>
<td>36 (10-82)</td>
</tr>
<tr>
<td>Patients with ischemic brain volume larger than the control range, %</td>
<td>NA</td>
<td>39</td>
<td>NA</td>
<td>65</td>
</tr>
</tbody>
</table>

Abbreviations: IQR, interquartile range; NA, not applicable; TBI, traumatic brain injury.  
* Mann-Whitney test between all patients with TBI and control participants.  
* b Within 24 hours postinjury.  
* c Days 2 through 5 postinjury.  
* d Days 6 through 10 postinjury.  
* e Kruskal-Wallis test between all groups, with the subsequent post hoc Dunn test surviving correction for multiple comparisons (P < .007) between early and intermediate points after TBI. Comparisons that did not meet this threshold are not shown.  
* f Kruskal-Wallis test between all groups, with the subsequent post hoc Dunn test surviving correction for multiple comparisons (P < .007) between early and late points after TBI. Comparisons that did not meet this threshold are not shown.  
* g The percentage of patients with ischemic brain volume larger than the maximum value found in control participants (20 mL) are shown.
quantified across ROIs in individual patients using the Spearman rank test, with high ρ values providing evidence of preserved flow-metabolism coupling. While there was substantial interparticipant heterogeneity, patients with TBI (median ρ, 0.44 [IQR, 0.25-0.64]) showed lower correlation coefficients than control participants (ρ, 0.75 [0.67-0.86]; P < .001; eFigure 5 and eTable 5 in the Supplement).

Ischemia
Oxygen extraction fraction showed a nonlinear association with CBF, with substantial within-participant and between-participant heterogeneity (eFigure 6 in the Supplement). Within 24 hours, OEF increased sharply when CBF was less than 25 mL/100 mL/min (the lower CBF limit in control participants), suggesting cerebral ischemia. Across all points, while some regions showed increases, OEF tended to plateau at approximately 45% when CBF was less than 25 mL/100 mL/min. While IBV elevations were most common within 24 hours of injury (median [IQR] IBV in early imaging, 24 [4-42] mL) and were not associated with intracranial hypertension (Table 2; Figure 3). All patients had CPP greater than 60 mm Hg. Ischemic brain volume was not associated with CPP (ρ, -0.06; P = .60) and did not differ in those who underwent craniectomy (median [IQR], 11 [5-28] vs 10 [4-49] mL; P = .75) or barbiturate coma (median [IQR], 24 [5-67] vs 10 [4-37] mL; P = .36). Within 24 hours, IBV was associated with worse outcomes, as quantified via the GOS (ρ, -0.63; P = .006), but there was no association across the whole cohort (ρ, -0.06; P = .71). After TBI, there was no association between CBF and Paco2 (ρ, -0.39; P = .09) or CBF and IBV measured during PET (ρ, -0.17; P = .10) or within separate temporal cohorts.

Bedside Monitors of Brain Oximetry
We had 67 PET sessions with SJVO2 and 38 with BTPO2 monitoring. We found no association between IBV and SJVO2 (Figure 3). Within the first 24 hours, there was some evidence of an inflection point at an SJVO2 of approximately 60%; when the level was less than this, IBV showed progressive
Spatial and Temporal Pattern of Ischemia and Abnormal Vascular Function Following Traumatic Brain Injury

Discussion

Ischemic Burden

After TBI, CBF shows a triphasic pattern, classically described as consisting of early hypoperfusion (<24 hours), hyperemia (1-3 days), and vasospasm (after 3 days). Most previous analyses have been based on indirect CBF measurement, typically using transcranial Doppler ultrasonography. Imaging has not commonly used CMRO2 measurement, making it impossible to differentiate ischemia from hypoperfusion appropriately coupled with hypometabolism. Our data show that classical ischemia (diagnosed by the incontrovertible metabolic signature of high OEF) is seen in many patients within 24 hours of injury, can...
be observed later, and can occur despite optimization of CPP, $P_{aco_2}$, and ICP.

Other groups have found less consistent evidence of classical ischemia using $^{15}$O PET in patients with TBI. Several of these studies focused on patients with less severe TBI at later points, with less significant physiological derangements, and for a limited period. Some specifically addressed contused brain and provided little data on cerebrovascular pathophysiology in structurally normal brain, which often constitutes the largest tissue compartment after TBI. Additional contributors to this discrepancy include the use of bolus, as opposed to our use of steady-state PET techniques, and different approaches to quantifying ischemic burden (ROI vs voxel-based methods). Our data are in keeping with the frequent detection of cerebral ischemia and infarction after TBI, both with antemortem imaging and postmortem neuropathology.

Hyperventilation can result in acute CBF reductions, with increases in OEF and reductions in CMRO$_2$ in some patients. However, IBV in this cohort was not associated with steady-state $P_{aco_2}$, perhaps because hyperventilation was being titrated to monitors of cerebral oximetry (SIVO$_2$, or BTPO$_2$) and used to control intracranial hypertension. Alternatively, hyperventilation-induced ischemia may resolve over time as extracellular pH in the brain normalizes. Although this compensation is incomplete for CBF reductions (as opposed to CBV), it may make it difficult to detect ischemia at steady-state low $P_{aco_2}$ levels (which was the case in the participants in this study).

**CBF-OEF Associations**

Reductions in CBF to less than the normal range resulted in sharp OEF increases within the first 24 hours. However, such OEF increases were not systematically achieved by similar CBF reductions at later points, which could imply a failure of oxygen extraction or use. Microvascular dysfunction and diffusion hypoxia are known to occur in a normal-appearing brain of a patient with TBI and can limit the ability to increase OEF. Similarly, oxygen use may be prevented by mitochondrial dysfunction, either because of structural mitochondrial damage or competitive inhibition of the mitochondrial respiratory chain by nitric oxide. Finally, persistent CBF reductions may result in patchy necrosis or selective neuronal loss. The overall CBF in such heterogeneous regions may be low but appropriate for the remaining viable tissue.

**Abnormal Flow Metabolism Coupling and Bedside Monitoring of Ischemia**

These data show generalized abnormalities in flow-metabolism coupling, with weaker associations between CBF and CMRO$_2$ in patients with TBI compared with control participants. A high CBF/CMRO$_2$ ratio implies hyperemia and was most prominent 2 to 5 days postinjury. These findings are consistent with transcranial Doppler ultrasonography data, but our additional CMRO$_2$ measurement allows confirmation that these represent true hyperemia. We documented between-participant heterogeneity, but also within-participant heterogeneity, since regions with high and low OEF often coexisted within the same patient. This heterogeneity may confound bedside monitoring, since global methods (SIVO$_2$) may dilute and miss focal pathophysiology, while focal monitors (BTPO$_2$) are critically dependent on sensor position. We saw some evidence of an SIVO$_2$ threshold of approximately 60%, and at levels less than this, IBV increased (particularly within 24 hours of TBI). However, many patients with high IBV had SIVO$_2$ values that were substantially greater than this threshold level, and use of the typical SIVO$_2$ less than 50% would have missed all but 1 patient with critical brain ischemia. We found no reliable association between BTPO$_2$ and IBV. In fact, many participants with low BTPO$_2$ values (<15 mm Hg) did not show IBV increases. Our inference is that focal BTPO$_2$ monitoring is not reliably associated with the global or regional burden of ischemia.

**Cerebral Ischemia and Outcome**

As demonstrated previously, $^{4}$ IBV within the first 24 hours after TBI was associated with GOS, underlining the clinical significance of early ischemia. The lack of correlation between later IBV and GOS raises the possibility that later ischemia is better tolerated, but it is more likely that other energy failure mechanisms (such as diffusion hypoxia and mitochondrial dysfunction) make greater contributions to outcome at these points.

**Association of CBV With ICP**

Previous reports, using estimates based on a combination of xenon and perfusion CT, reported reduced CBV in patients with TBI. The direct CBV measurement in this report shows that it was consistently raised, but the contribution to ICP elevation was complex. Patients with intracranial hypertension showed lower CBV values than those with ICP values of 20 mm Hg or less, but this unexpected association was likely attributable to lower $P_{aco_2}$ in patients with intracranial hypertension, in whom hyperventilation therapy was used. Despite this, their CBV values remained significantly greater than those of control participants, suggesting that CBV elevations continued to contribute to intracranial hypertension. While cerebral edema is an important driver of intracranial hypertension, we show that CBV increases also contribute, providing a physiological basis for interventions aimed at reducing the vascular contribution to intracranial volume.

**CBF/CBV Associations**

We found regional differences in CBF/CBV in patients with TBI, replicating past results from control participants. Since experimental studies suggest a linear association between CPP and CBF/CBV, we calculated CBF/CBV divided by CPP to account for lower CPP values in individuals with TBI. However, CBF/CBV divided by CPP remained lower in individuals with TBI (Table 2), suggesting that simple autoregulatory vasodilatation could not explain this finding. Reduced CBF/CBV in individuals with TBI may represent impaired dilatation of precapillary resistance units (resulting in low CBF) and/or a disproportionate increase in (probably venous) capacitance in the cerebrovascular circuit. These inferences are concordant with past TBI data, which show that the effect of hyperventilation on CBV (and hence ICP) is tran-
sient, while the CBF reductions it produces are dominant and sustained.39

Limitations
Although our data were collected prospectively in accordance with a common protocol, this was a retrospective collation with nonconsecutive recruitment driven by convenience and logistics, which makes generalizability difficult to assess. Imaging was not possible on days on which patients were too unstable or scanners were unavailable. Although data were acquired over 16 years, all patients were recruited after the introduction of the Cambridge ICP/CPP protocol, and any changes in physiological targets over the recruitment period were relatively small and have been detailed in a recent publication.44 Systemic physiology during each scan is available and explicitly summarized in Table 1. We used global, regional, and voxel-based analyses, but each has potential pitfalls; global and region-based measures may miss voxel-level pathophysiological heterogeneity, whereas voxel-based approaches are more susceptible to noise. While this was, to our knowledge, the largest single-center 15O PET study in individuals with TBI (90 scans), ideally an assessment of the temporal patterns of physiology would make use of sequential studies within participants. However, such studies are difficult to undertake and limited by considerations of patient safety and stability. Consequently, the sample available for analysis represents the data that were obtainable in this context. We did have 17 patients in whom PET were available on more than 1 occasion. This temporal patterns in this subset broadly replicate those of the overall cohort, suggesting the larger data set provides a useful representation of temporal trends in regional physiology. Further analysis, using a mixed-effects model that accounted for the inclusion of data from multiple ROIs within each participant, confirmed the association of time postinjury with regional cerebrovascular variables in comparison with data from control participants. Finally, this analysis explored pathophysiology in structurally normal tissue to examine the brain at risk of evolving injury, and hence it does not provide a complete picture of all pathophysiological tissue compartments after TBI.

Conclusions
In a large cohort of individuals with TBI, 15O PET imaging shows systematic changes in cerebrovascular physiology that have direct clinical relevance. Early ischemia (<24 hours) occurs in approximately two-thirds of patients, is detectable up to 10 days postinjury, and is not limited to patients with intracranial hypertension. We found significant outcome associations with ischemia that occurred early but not after 24 hours, implying that other pathophysiological mechanisms of energy failure may be dominant during later phases of the disease narrative. We demonstrate substantial pathophysiological heterogeneity within patients, with ischemia and hyperemia coexisting in different brain regions, reflecting abnormalities in flow-metabolism coupling. Global (SjVO2) or focal (BTPO2) measures of cerebral oximetry provide data that guide clinical management, but physiological heterogeneity dictates that these should be interpreted with caution. Cerebral blood volume is consistently increased in patients with TBI and remains higher than control values even in patients with intracranial hypertension, despite lower PaCO2 being used to manage ICP. These data are in keeping with CBV increases as a contributor to intracranial hypertension. However, there may be disassociation of CBF/CBV homeostasis, with disproportionately high CBV seen across the entire postinjury period despite low CBF. Such physiological disassociation, along with the regional variations in physiology and the inconsistent associations with monitoring that we demonstrate in this study, may inform clinical management of patients with TBI.


